



Neural Interfaces

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Clinical applications

Trauma



Neurodegenerative conditions



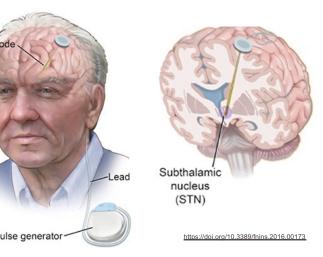
NX-422 ©LSBI

Clinical applications

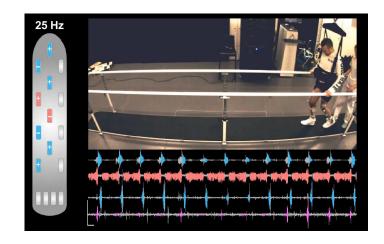
diagnostic



intervention



rehabilitation



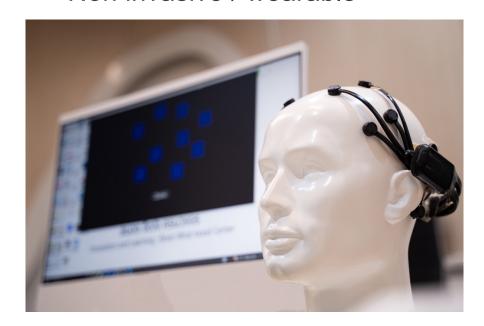
MRI

deep brain stimulation

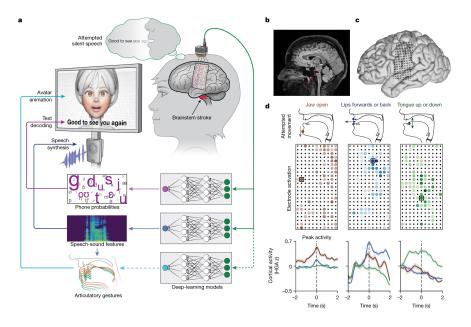
robotic assistance

Two classes of neurotechnology

Non invasive / wearable



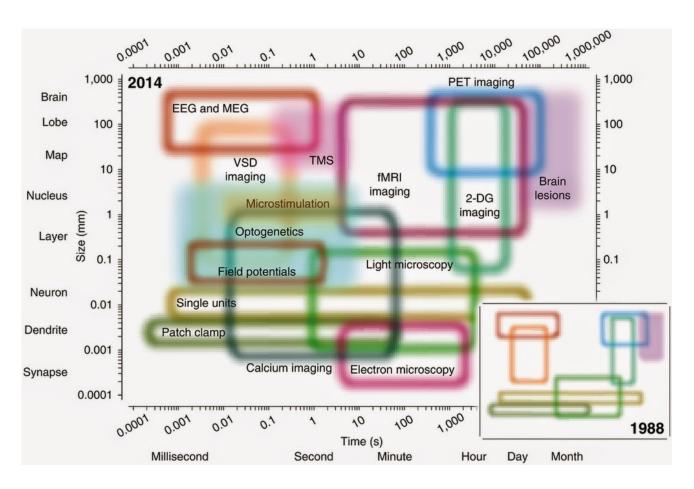
Invasive



Nature 2023, UCSF

Functional representation of neural signals

- Spatial resolution
- Temporal resolution
- Invasiveness



MRI Magnetic resonance imaging -

Reference imaging

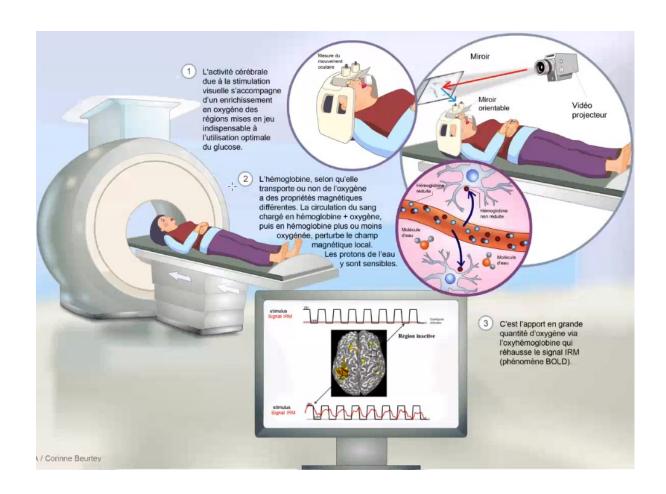
- Magnet
 - 1.5T
 - 3T
 - 7T
 - 11.5T / research



Siemens Healthineers

EPFL MRI and fMRI

- Anatomy
- Functional imaging
 - observation upon stimulation
 - BOLD (blood oxygen level dependence)



EEG imaging

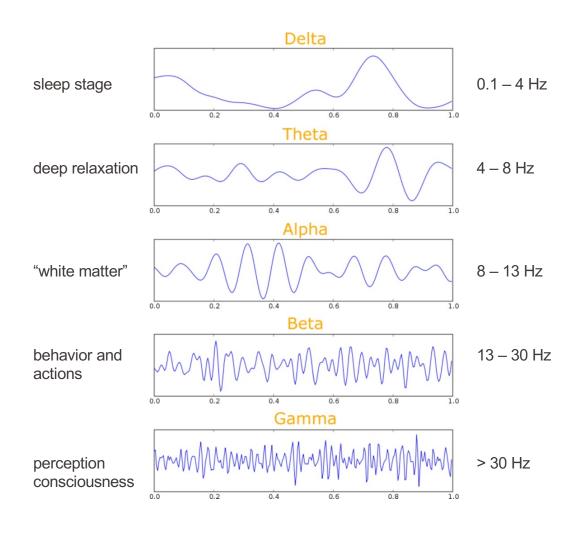


Brain Products

Electroencephalography **EEG**

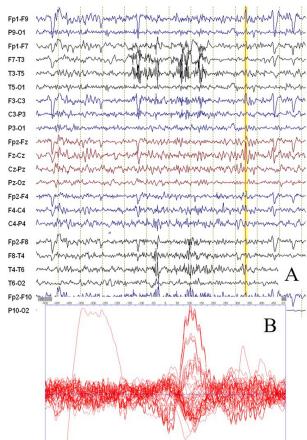
5 – $300~\mu V,$ < 100~Hz

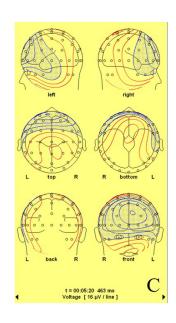
Brain waves



Frontal epilespy

- A. High resolution EEG data
- B. Interictal event with the 64 channels superimposed
- C. Surface amplitude cartography
- D. Epileptic source localisation



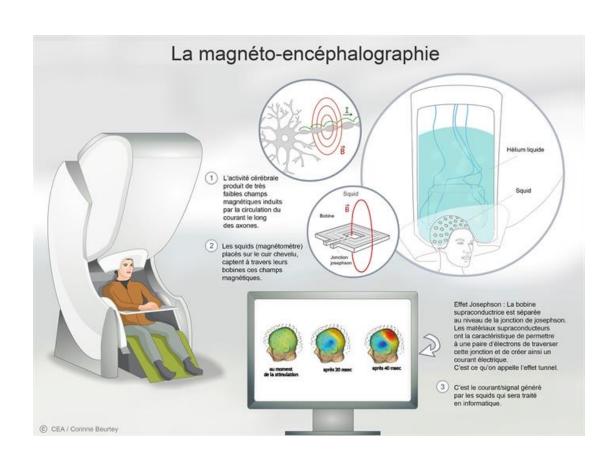




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Magnetoencephalography MEG

 monitoring magnetic field generated through brain activity



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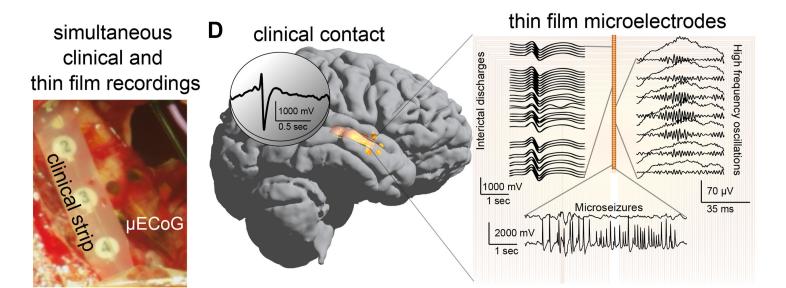
Electrocorticography ECoG

- Diagnostic:
 - Localisation of epileptic sources
 - Guide for tumor resection
 - Diagnostic for brain trauma
- Intraoperative or short-term (<30 days) monitoring

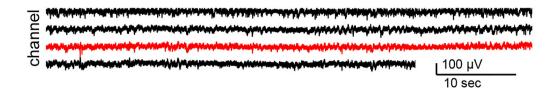


EPFL S

Signals vs electrode size



Clinical electrodes Θ=1mm, 1cm inter-electrode

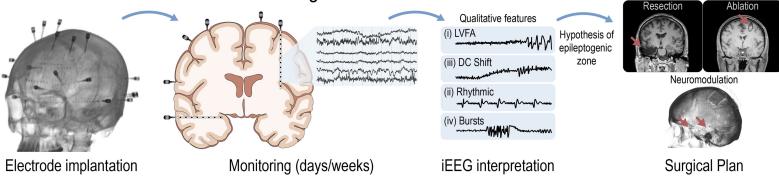


Micro-electrodes Θ = 50μm, 1mm inter-electrode

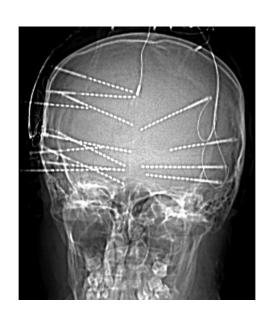
https://doi.org/10.1016/j.nec.2023.09.003

sEEG – stereo EEG

Clinical workflow of invasive monitoring

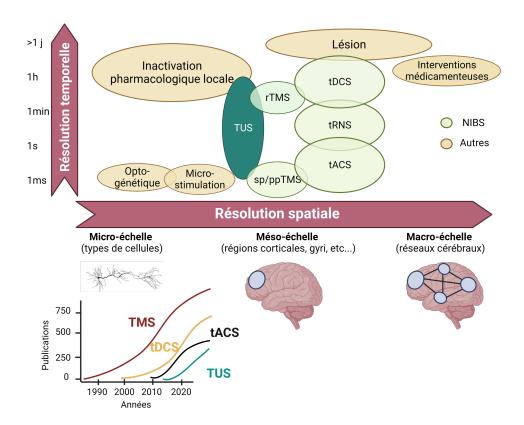


https://doi.org/10.1093/brain/awad007



J Neurosurg Pediatr vol 28 • 2021 404-15

Non invasive neuromodulation



t-. transcranial

DCS: Direct Current Stimulation

ACS: Alternative Current Stimulation

RNS: random Noise Stimulation

TMS: Transcranial Magnetic Stimulation

TUS: Transcranial Ultra-sound Stimulation

NY ADD @ CCL XIA

EPFL

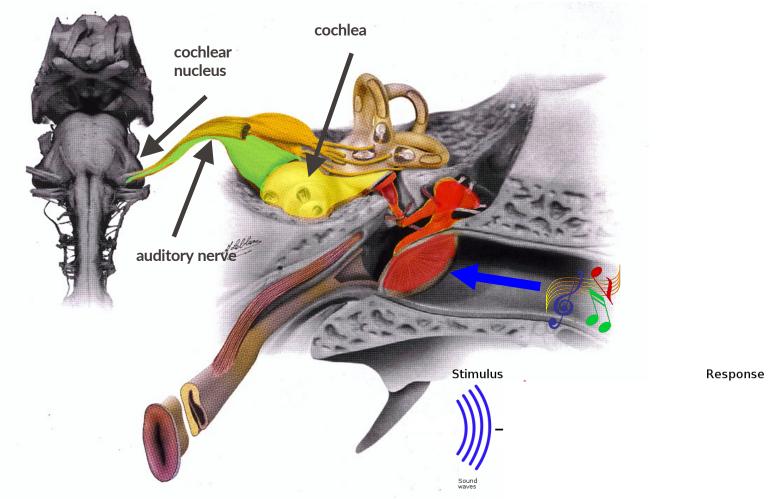
Invasive neurotechnologies

Cochlear implants

Deep brain stimulation

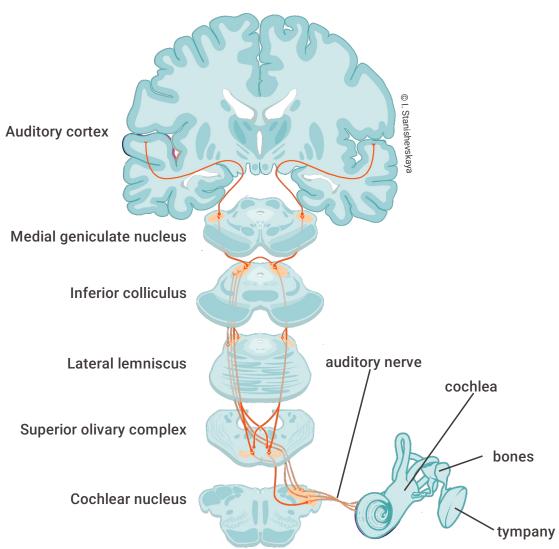
Stimulation of the spinal cord



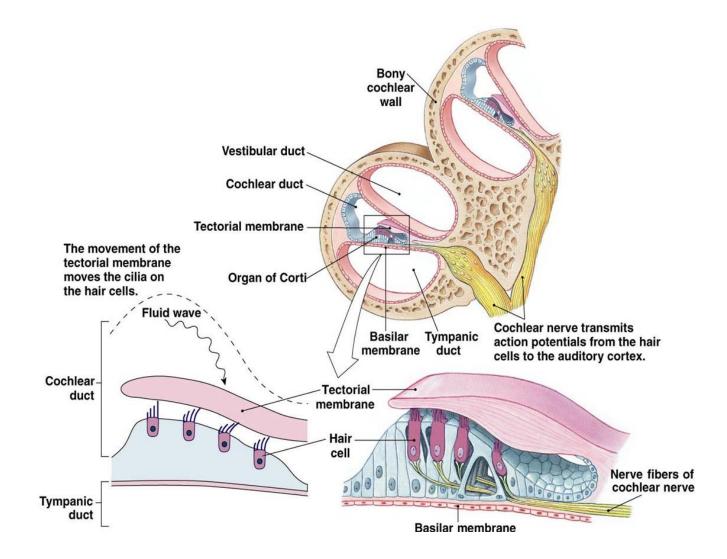


Original diagram by Tim Gollisch, Andreas M. V. Herz, and Public Library of Science. Converted to SVG by lain 03:57, 12 June 2006 (UTC) Permission

Auditory circuits



The cochlea



Cochlear implants *History*

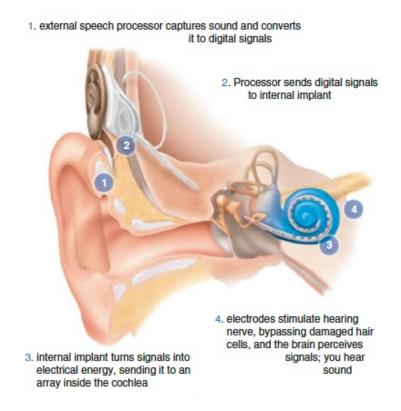
- First "experience": Alessandro Volta (1800)
 - Electrical stimulation evoke auditory sensation in humans
- 1957 electrical stimulation of hearing in 2 deafened patients
- 1960s-1970s multiplied efforts in the USA
- 1984: FDA approves the first cochlear implant (many others ensue)

Main players today:

- Med-El Corp., AU; Cochlear Corp., AUS; (Advanced Bionics) Sonova Holding, CH
- audiological criteria for cochlear implantation:
 - from bilateral total deafness (<110 dB HL) in the early 1980s
 - to severe hearing loss (>70db HL) in the 1990s,
 - then to current suprathreshold speech based criteria (< 50% open-set sentence recognition with properly fitted hearing aids).

Cochlear implants





A long-term interface

- Exceptional constraints on life-time, reliability of the interface
 - Implantation in new-borns
- Implantable electronics: as simple as possible
 - Transmitter of signals received from external device to the electrodes
 - 12-22 channel electrode
 - "no upgrade" over time of the implanted hardware
- External speech processor
 - Complex signal processing
 - Positioned behind the ear
 - Energy source (battery)



Surgical positioning

- Difficulty due to configuration of bones around the cochlea
- Proximity of facial nerves
- Alignment of the external and internal coils
 - Implanted magnet (issue with MRI)



EPFL Implantable electronics

- Titanium housing providing hermetic seal to implantable electronics
 - Must be as thin as possible
 - Limited protrusion under the skin
 - Minimal skin erosion
 - Inductive coupling for power transfer
 - Induction coil outside of the casing
 - mm distance between coils
 - Alignment of coils
 - External batteries

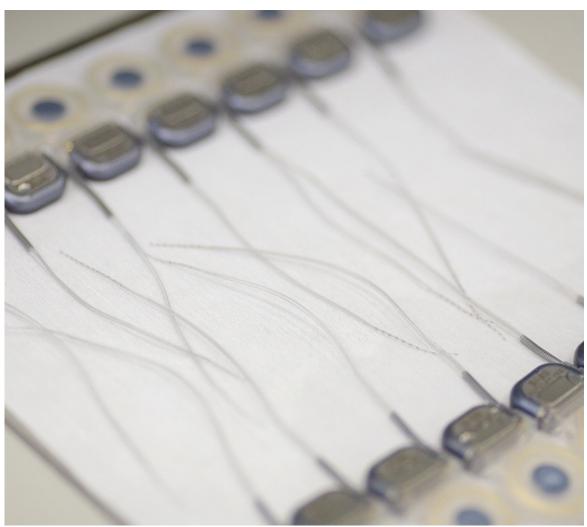
Connectors

- Non detachable lead cable from housing
- Challenges of number of contacts and hermeticity
- One company: Bal Seal Engineering Inc.





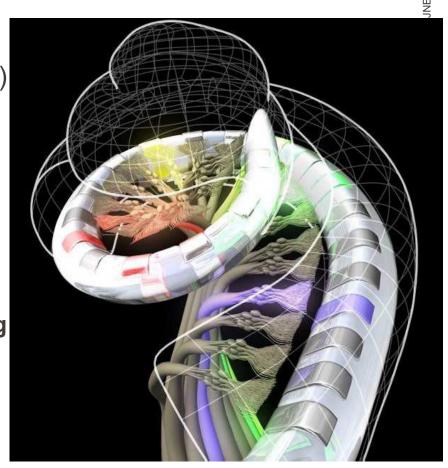
Implantable interface



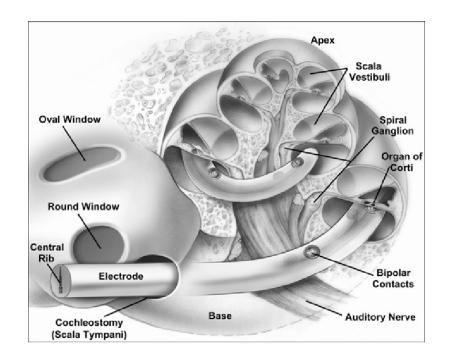
Cochlear Electrodes

Invasive electrodes (surgical positioning)

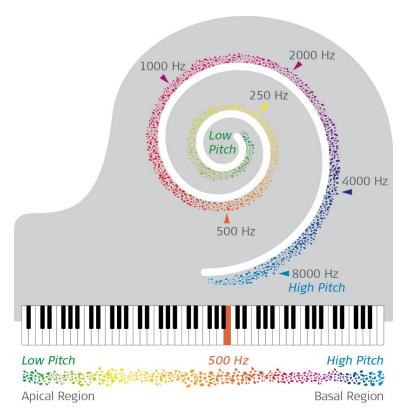
- Electrode contacts
 - non-insulated surface
 - Metal: Platinum
- Insulated wires
 - gathered in a coiled cable or a flat ribbon
 - Materials: Platinum-Iridium 90/10
 with Teflon insulating coating
- > Embedded in **silicone** to form the lead



The cochlear implant

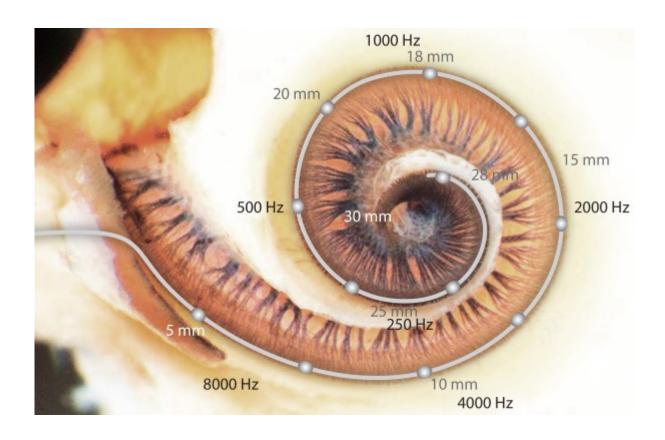


https://www.youtube.com/watch?v=bDx12M5u4uY#t=45



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Accessing the cochlear tonotopy



The diameter of the cochlea canal is about 1mm at the widest Radius of curvature: ~ 4mm

Cochlear implant







Enables speech understanding in quiet and some noisy environment

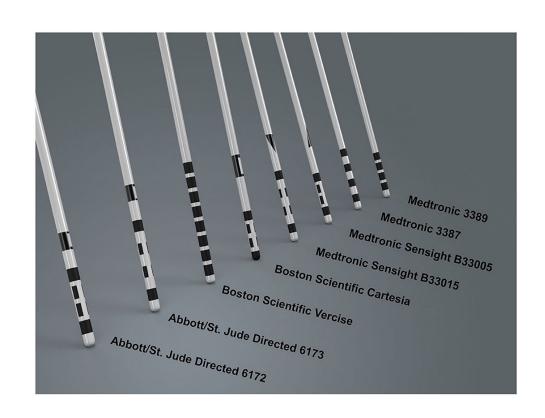
Deep brain stimulation DBS

- Electrodes
- Cable (lead)
- Implanted electronics
- Control
- Recharge



DBS electrodes

- DBS lead (Electrodes)
- Extension
- Neurostimulator
- Adjustment



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DBS Implantable Pulse Generator (IPG)

- DBS lead (Electrodes)
- Extension
- Neurostimulator
- Adjustment



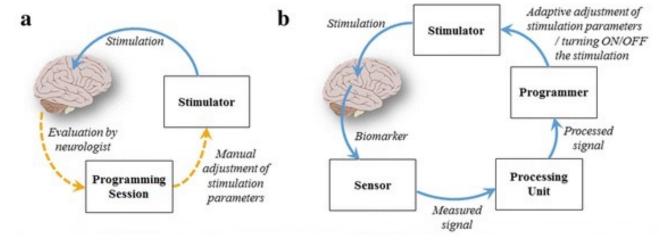


Select and adjust

- DBS lead (Electrodes)
- Extension
- Neurostimulator
- Adjustment



DBS & closed loop systems



introduced in 2000s

Realtime adjustment of stimulation parameters as a function of biological metrics

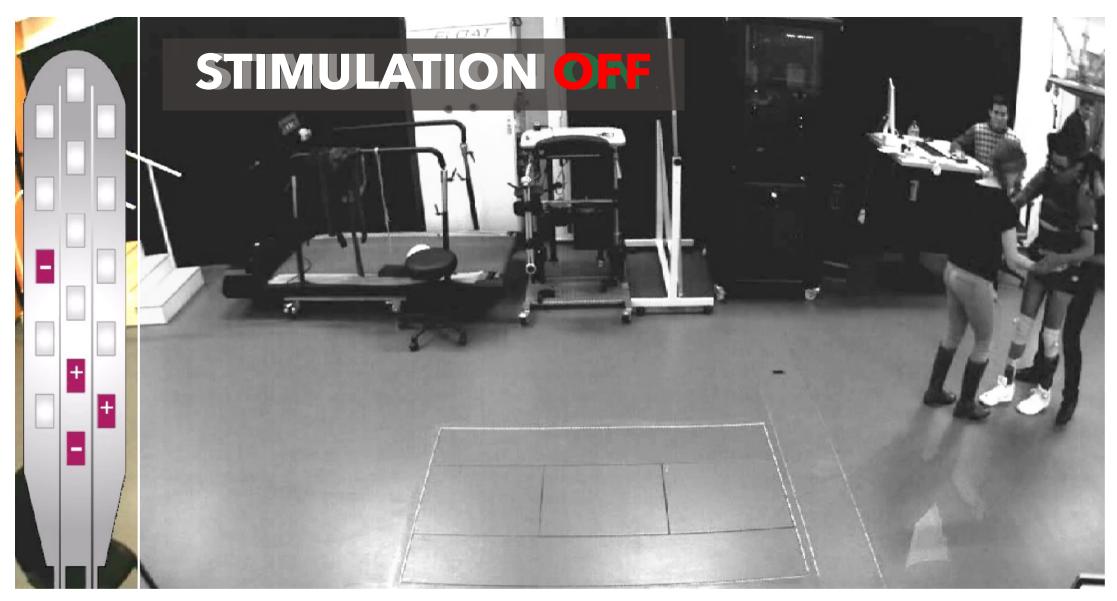
■ NX-422 ©LSBI

Stimulation of the spinal cord

Spinal cord injury

G. Courtine, J. Bloch EPFL/CHUV/UNIL

Rowald et al. **Nature Medicine** 2022



G. Courtine, J. Bloch EPFL/CHUV/UNIL

Human-machine interfaces

upper limb movement following paralysis

BROWN

Nature 2012

Tactile sensation with a robotic hand



Science Trans. Med. 2014

Speech restoration through a BCI and an avatar



Nature 2023

Biological metrics (1/2)

- The aqueous internal environment
 - Water: 55 75% in weight
 - Intercellular fluid (1/3) and extracellular fluid (2/3)
 - Body temperature: 37°C
- Biological fluidics
 - Bulk flow: transport with the carrying medium (blood, air)
 - Passive diffusion: concentration gradient

Biological metrics (2/2)

Biological electricity

- Movement of ions across the membrane of the cells → ionic currents
 - Membrane potential E_m, between -60mV and -90mV
- Excitable tissues can generate action potentials
 - Transient depolarization of the cell as a result of ion channel activity
 - Action potentials transmit information to nerve cells
 - Action potentials trigger contractions in muscle cells

Biological devices

Actuators: Muscles

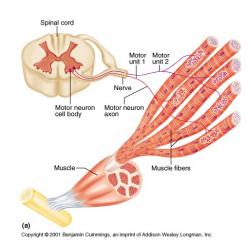
- Soft tissues, which change size and shape
- Produce force and motion
- Skeletal / cardiac / smooth (involuntary)

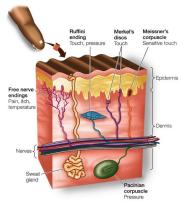
Sensors

- Mechanoreceptors (touch)
- Chemoreceptors (taste)
- . . .

Processor

- Neural circuits
- Peripheral nerves / spinal cord / brain





LIFE 8e, Figure 45.6

E THE SCIENCE OF BIOLOGY, Eighth Edition © 2007 Sinauer Associates, Inc. and W. H. Freeman & Co.

Brain vs CPU

	Whole brain	CPU
weight	1.4 kg	< 100g
power	~22W	> 25W
units	10 ¹¹ neurons	10 ⁸ transistors
Glial cells	~3 x neurons	
connections	10 ¹⁵	> 10 ¹⁰
wiring	8 million of km of axons	~ 100 km

Based on Intel Core i7-1260U

Supercomputers vs the brain

- the human brain: ~85 billion neurons with 1/10'000 connectivity
- the brain computing: very hard to estimate
 - 1 10 petaFLOP/sec, maybe 1 exaFLOP/sec and under 50W power
- Supercomputers
 - 1960:
 - IBM7030 Stretch: > 1 million instruction per second
 - 2012:
 - IBM Blue Gene Q ® 16 petaFLOP/sec using 7.9MW (!)
 - 2024:
 - Train ChatGPT4 108 ExaFLOP/s, 50GWh

Important considerations when designing a neural interface

- Assess the topology of the medium to interface
- Assess the dynamics of the host medium
- Assess the function(s) of the biological tissue
- Define the form-factor and eventual range of compliance of the neural interface (application-driven)
- Select the appropriate device technology (including biocompatibility)
- Manufacture the required function and assess its reliability